

Introduction

- In MRI, we have two types of data acquisition
- Qualitative and quantitative
- The product of qualitative imaging is an image
- The product of quantitative imaging is not necessarily an image, it can be a graph or a specific curve or data

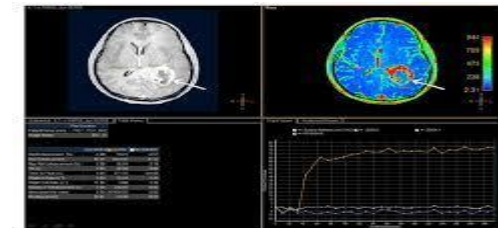
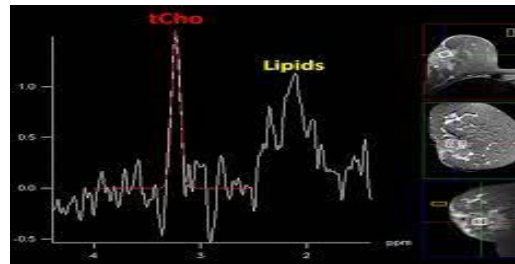
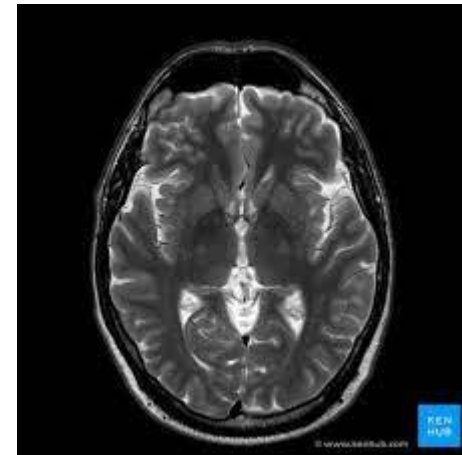
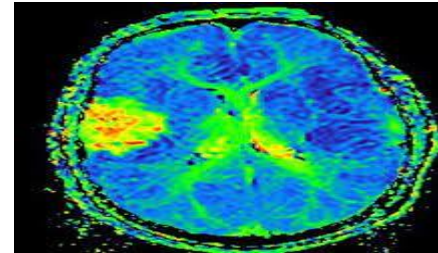
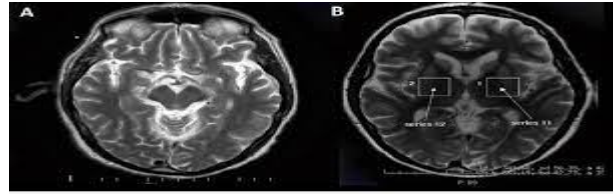


Figure 2: Axial semi-quantitative PFI image shows glioblastoma multiforme in the left parietal lobe (white arrow) with the significantly stronger perfusion parameters in comparison with the reference.

Introduction

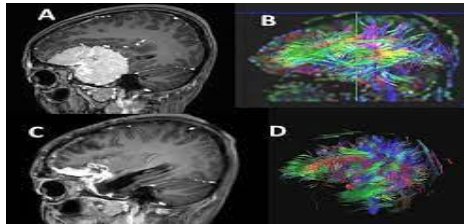
- Quantitative imaging included :

- DWI



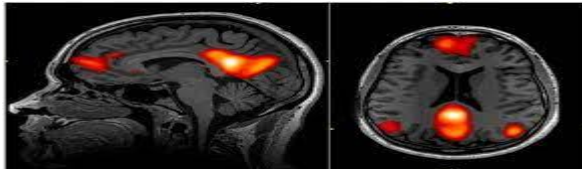
- PWI

- DTT

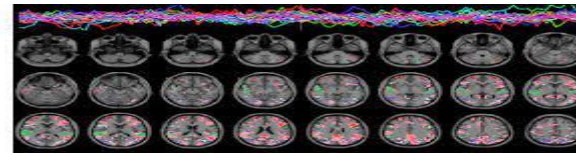


- DTI

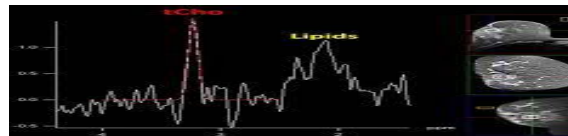
- BOLD



- Functional MRI

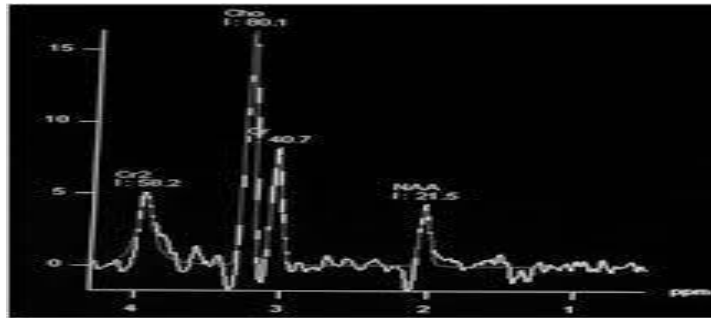


- MRS



Introduction

- **MRS**
- Finally, it gives us a curve or graph that should eventually be evaluated and converted into the data we want.

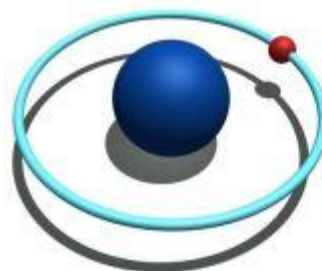
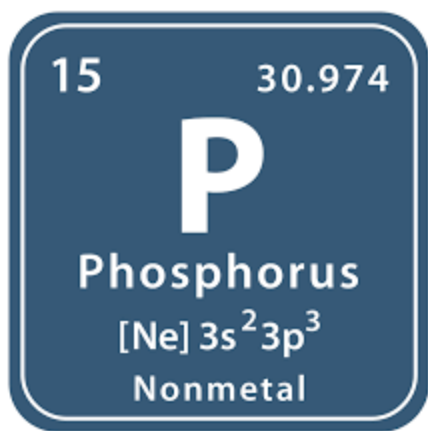


- Spectroscopy increases the diagnostic distance from 0 to 100 to 100%



Introduction

- In the devices that we currently have, with a field strength of 1.5 Tesla, imaging is done with two elements, hydrogen and phosphorus.

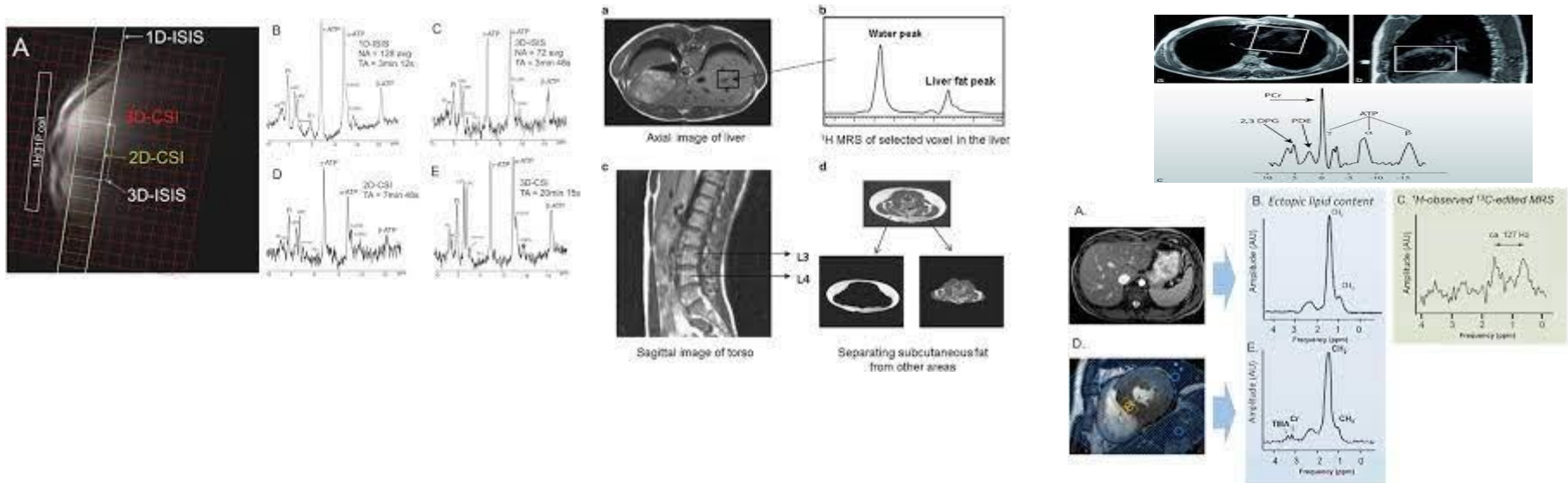


Introduction

In 1.5 Tesla more hydrogen can be used and the element phosphorus is usually set up for three Tesla devices and for some different organs.

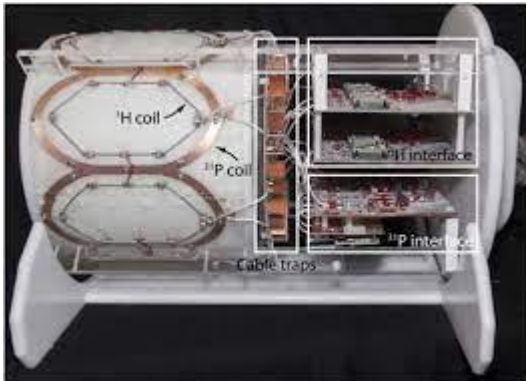


in practice Hydrogen can be used in all pulse spectroscopic sequences, but phosphorus is only used to examine the heart, liver, and muscles.



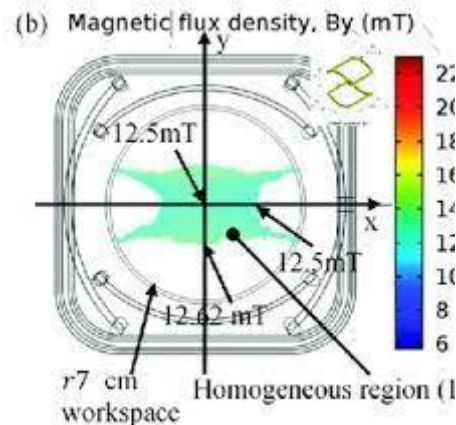
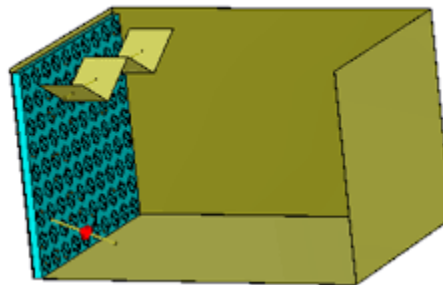
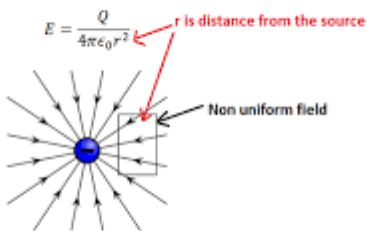
Introduction

The difference between imaging with hydrogen and phosphorus is that when using phosphorus we have a phosphorus coil that must be tuned to the device and is known and is usually used in devices with three Tesla and above.



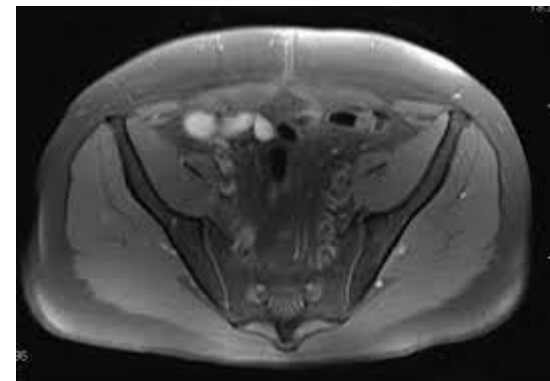
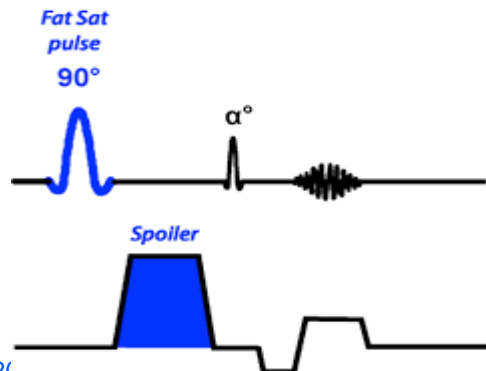
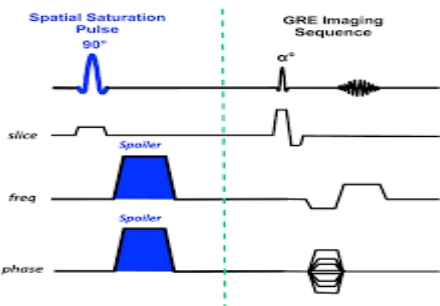
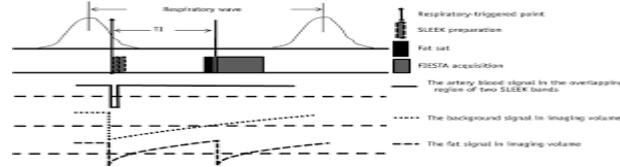
Introduction

- MRS is strongly related to the homogeneity and uniformity of the field.
- Designed for 1 Tesla and above devices and not lower than that



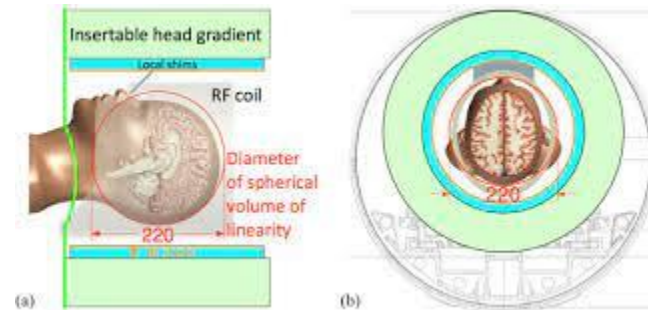
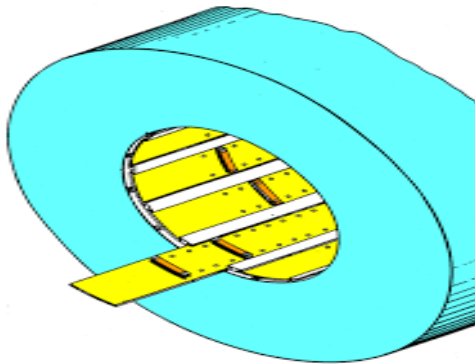
Introduction

- Used on devices above a Tesla when the magnet of device has uniformity and homogeneity and good tuning
- Spectroscopy is practically unusable if a metal or case sticks to the device that disrupts the homogeneity of the device.
- To check the homogeneity of the device, we must see how capable the device is in fatsat pulses
- It has good spectroscopic capability if it can perform fatsats evenly



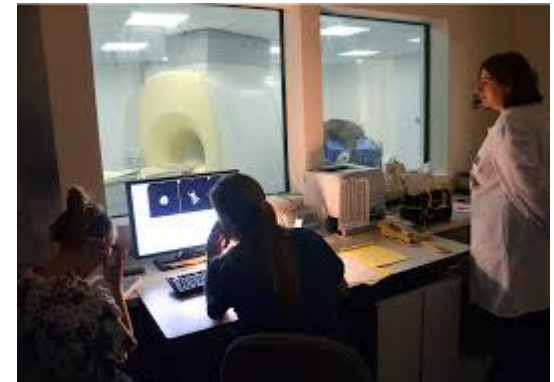
Introduction

- In siemens devices at our disposal, those designed for neurological centers.
- Two shimming samples are performed on them.
- Basic or standard or passive shimming for common devices for which passive shim and basic shim are performed
- Advanced shimming is for devices designed for neuroimaging and advanced shimming is performed on them.



Introduction

- The difference between a Siemens and a Philips magnet is that for the Philips, full shimming is done from the beginning and when the Siemens magnet is advanced, it equals the Philips.
- MRS is extremely sensitive to inhomogeneity and even opening and closing the magnet door can disrupt data.



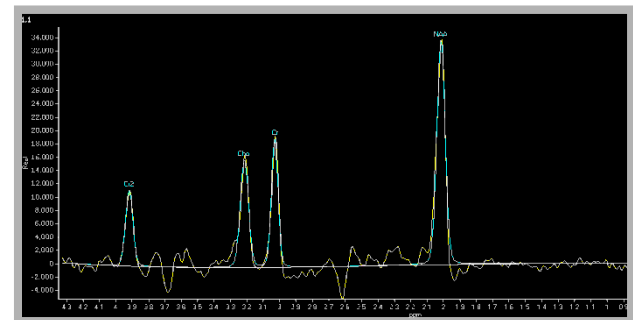
Introduction

What is Spectroscopy

- What is Spectroscopy?
 - Study of spectra

- What is a Spectrum?
 - A graphic representation of the distribution of energy emitted by a radiant source, arranged in order of frequencies

- What is MR spectroscopy?
 - Study spectra acquired on basis of the (N) MR principle

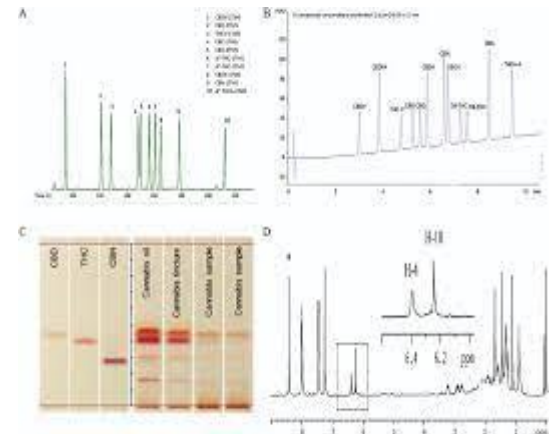
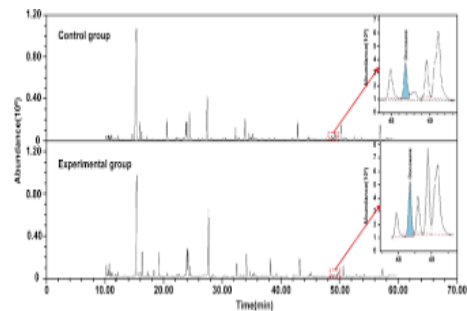
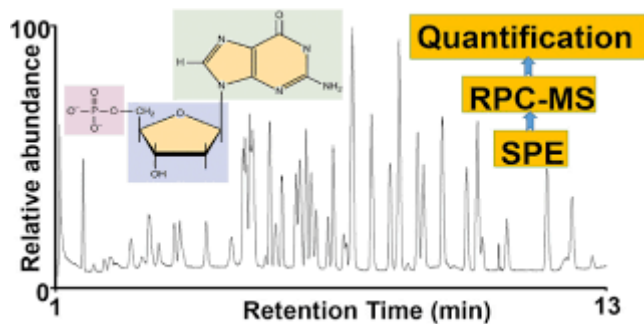


Introduction

- Magnetic resonance spectroscopy:
 - is an analytical method that enables:
 - the identification and quantification of metabolites in samples.

It differs from conventional MRI in that spectra provide physiologic and neurochemical state instead of anatomy

Metabolic changes may not be appear in anatomical image.



Introduction

MRS was first described in 1946 simultaneously by the Nobel Prize winner Edward Purcell.

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Introduction: MR Spectroscopy, history

- MR spectroscopy, or NMR spectroscopy is used since the 1950's as a non-destructive analytical method in chemistry and biochemistry
 - Small bore magnets
 - Very high field strength
 - In vitro measurements
- In 1986 MR spectroscopy was combined for the first time with an imaging system, the Gyroscan S15
 - Whole body scanner
 - High field strength
 - In vivo measurements

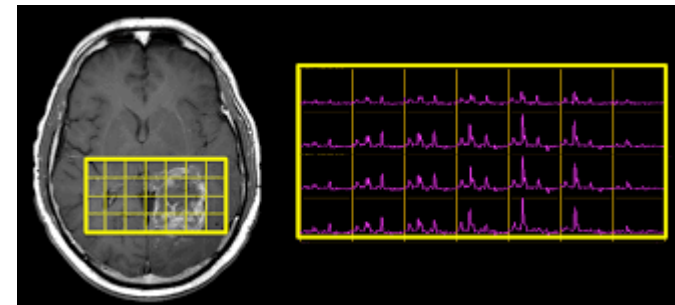
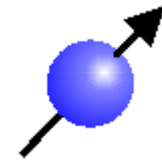


Introduction MR Spectroscopy

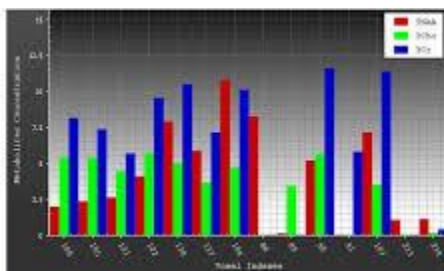
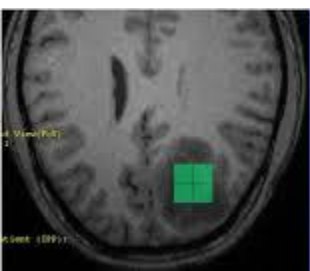
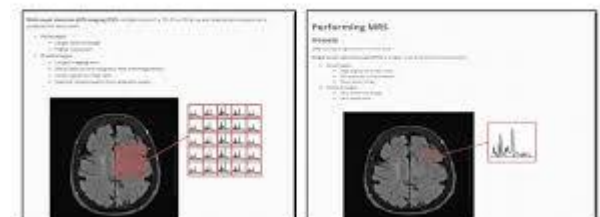
- MR spectroscopy (MRS) and imaging (MRI) share the same physical principles
- MRI is a way to produce a cross-sectional image based on proton (water) signal
- MRS is a method of gathering information about the chemical composition of the tissue of interest

The information is based on the difference in the resonance frequency of tissue metabolites: 'Chemical shift'

- Output:
 - * Spectrum per voxel
 - * Cross-sectional image based on a certain metabolite

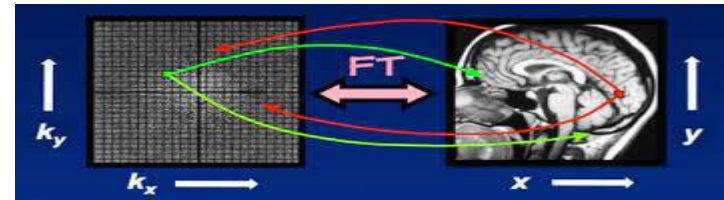
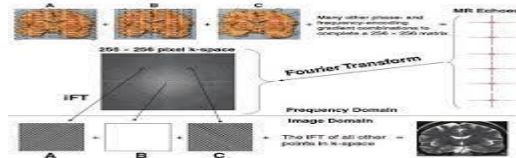


MR Spectroscopy

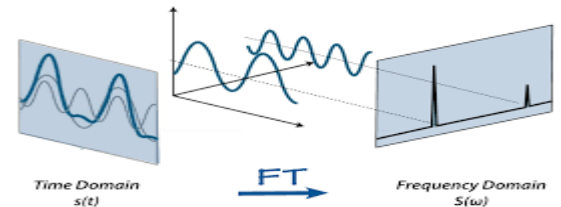
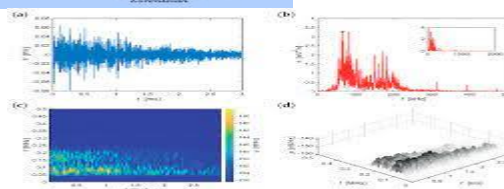
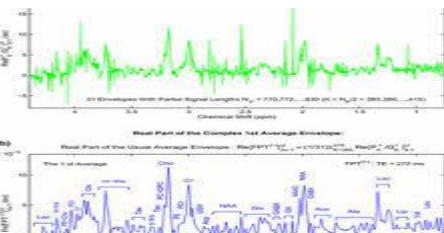


Introduction

- MRI & MRS are one and the same! Only differ in:
 - manner in which data is processed and presented - In MRI:
 - – signal obtained in a time unit
 - -generates image by Fourier transform & k-space •



- In MRS: Fourier transform of image signal generates a frequency spectrum of the image components

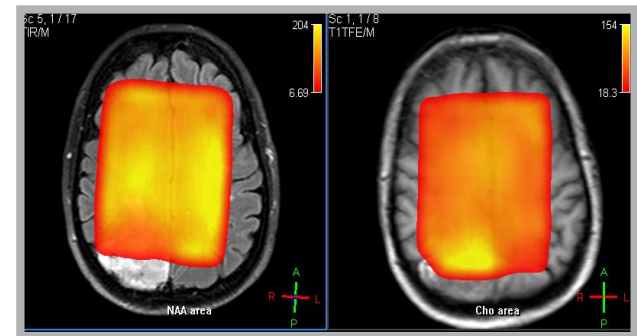
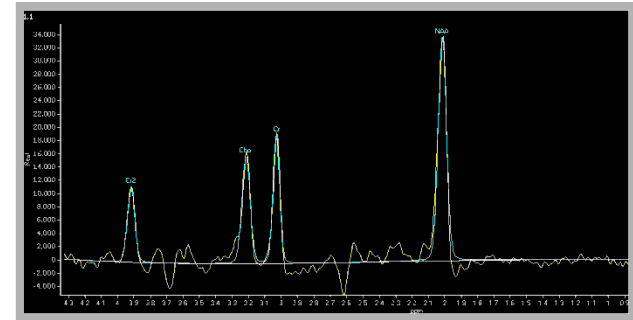


Introduction

MR Spectroscopy Results:

- Spectra
 - Graphical display of amplitude vs. frequency

- Chemical shift images
 - A representation of the amplitude (abundance) of a certain chemical (metabolite) over position (image)



Introduction

MR Spectroscopy vs. MR Imaging

	Spectroscopy	Imaging
Physical Phenomena	NMR	NMR
Applied Nuclei	^1H , ^{31}P , (^{13}C)	^1H
Magnetic Field	High	Low → high
Scan process	Collecting time signals (averaging)	Collecting different profiles
Presentation of information	1) Frequency spectrum 2) Spectroscopic Imaging	Cross sectional view of object
Application area	Metabolism Physiology	Anatomy Pathology
Gradients	1) (Single) Volume selection 2) Phase encoding (up to 3 directions)	Slice (volume) selection Frequency encoding Phase encoding (1 or 2 directions)
Shimming	Optimize homogeneity in the volume of interest (small)	Optimize homogeneity in the volume of interest (large)

Introduction:

MR Spectroscopy, Clinical use

- Research
- Increased use for diagnostic (and follow up) purposes
 - Spectroscopy as part of comprehensive neuro exam
 - * Tumors (differentiation, grading)
 - * Epilepsy (lateralization)
 - * Abscess
 - * Ischemia (stroke)
 - * Dementia/white matter diseases
 - * Neonatal applications
 - * Hepatic encephalopathy
 - Spectroscopy in body
 - * In principle everywhere in the body
 - * Prostate*****
 - * Liver
 - * Breast

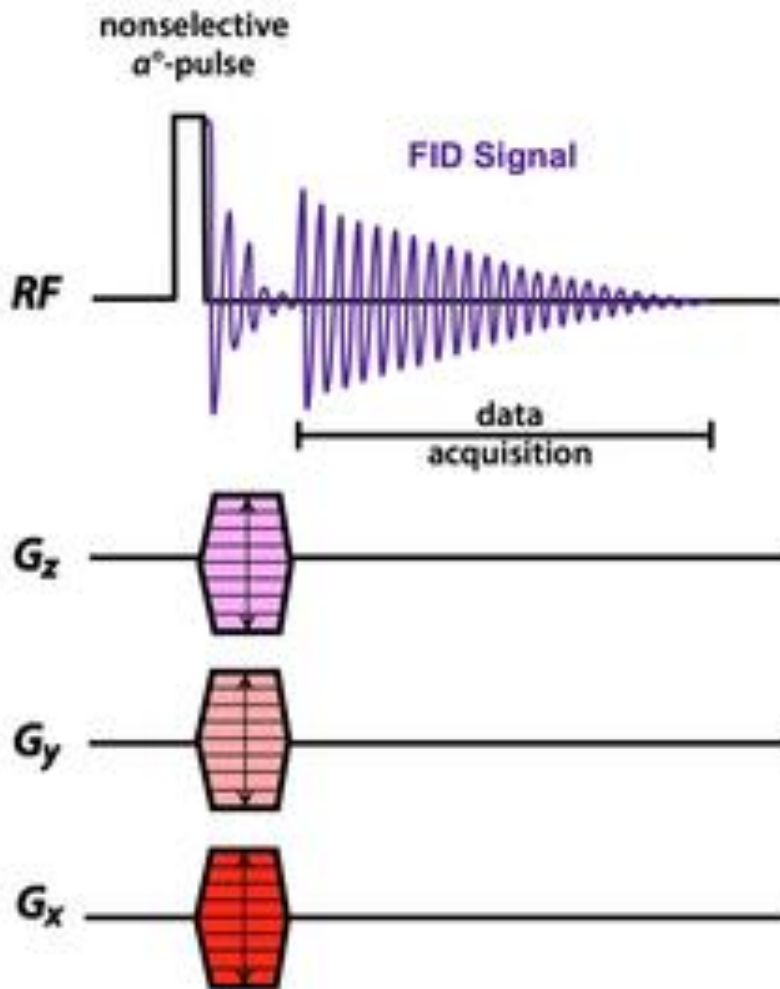
MR Spectroscopy

Metabolite sensitivity

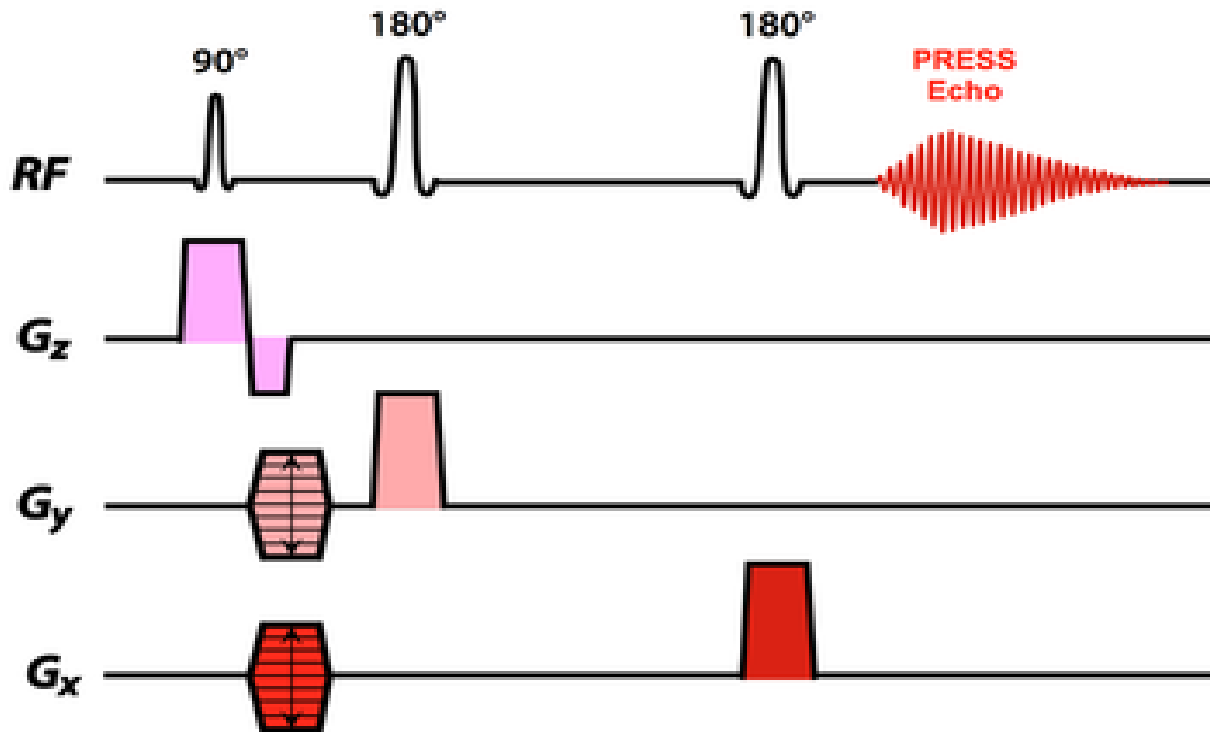
Chemical substance	Relative sensitivity (MR signal strength)	
	Percentage	Factor
Water	100 %	1
NAA, N-acetyl aspartate (¹ H spectrum)	0.03 %	3500
PCr, Phosphocreatine (³¹ P spectrum)	0.0007 %	140,000
¹³ C Spectroscopy	0.000002 %	50,000,000

Chemical Shift Imaging (CSI)

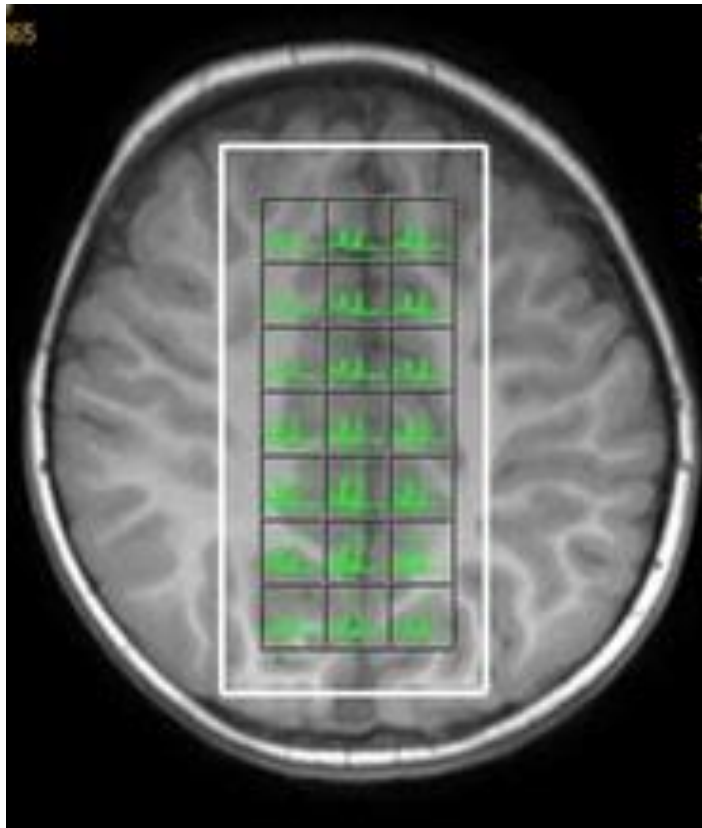
- *Chemical Shift Imaging (CSI)*, also known as *MR Spectroscopic Imaging (MRSI)*,



3D CSI sequence using nonselective volume excitation and stepped phase-encoding gradients along all three axes (common method for ^{31}P MRS)



2D-PRESS CSI sequence with slice-selective excitation pulses in 3 planes with stepped phase-encoding gradients along 2 axes (common method for ¹H brain MRS). Diagram has been simplified by leaving out preparatory water/fat saturation modules and crusher gradients)



2D CSI ^1H brain MRS

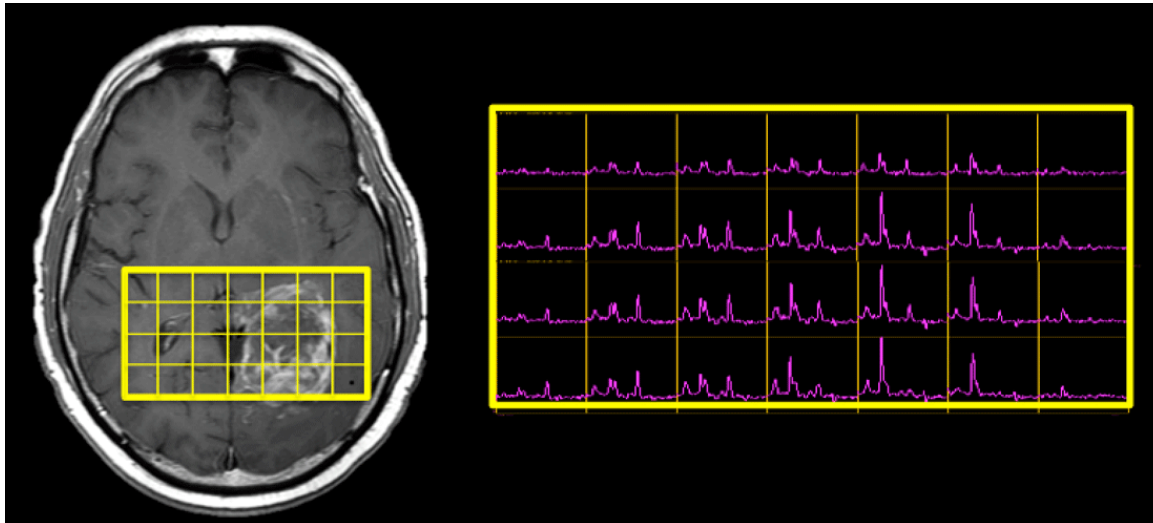
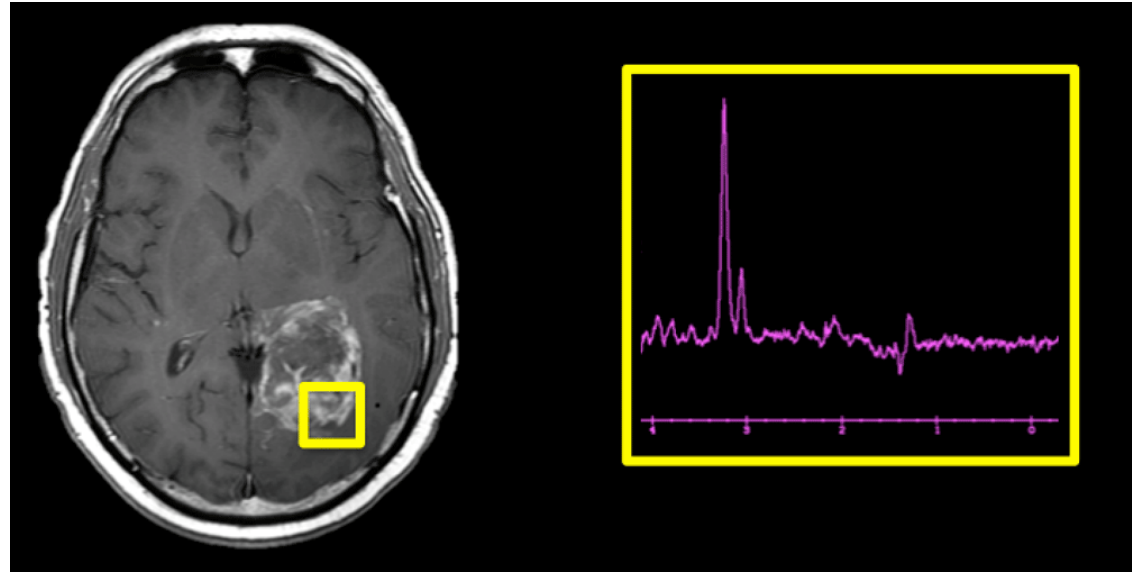
CSI offers both a larger total coverage area and higher spatial resolution than single-voxel methods.

The potential for a wide coverage area allows evaluation of large, heterogenous lesions, while smaller size of individual voxels is advantageous for small or irregularly shaped lesions.

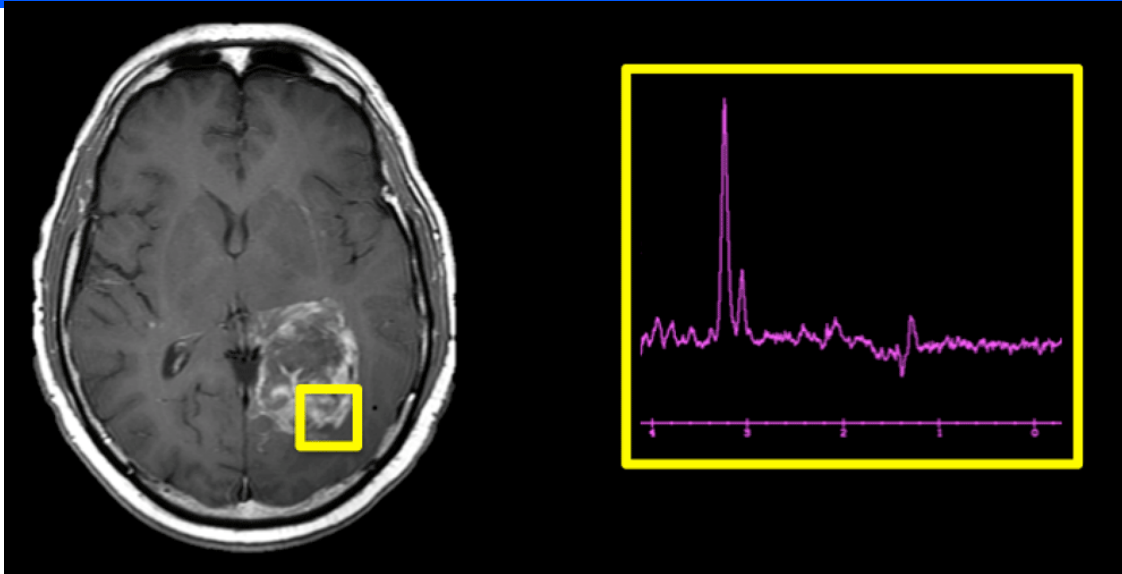
The major disadvantages of multi-voxel CSI include:

- 1) Longer set-up and imaging time;**
- 2) difficulties obtaining homogenous shim over the entire region;**
- 3) lower signal-to-noise and spectral quality for individual voxels;**
- 4) spectral contamination from adjacent voxels.**

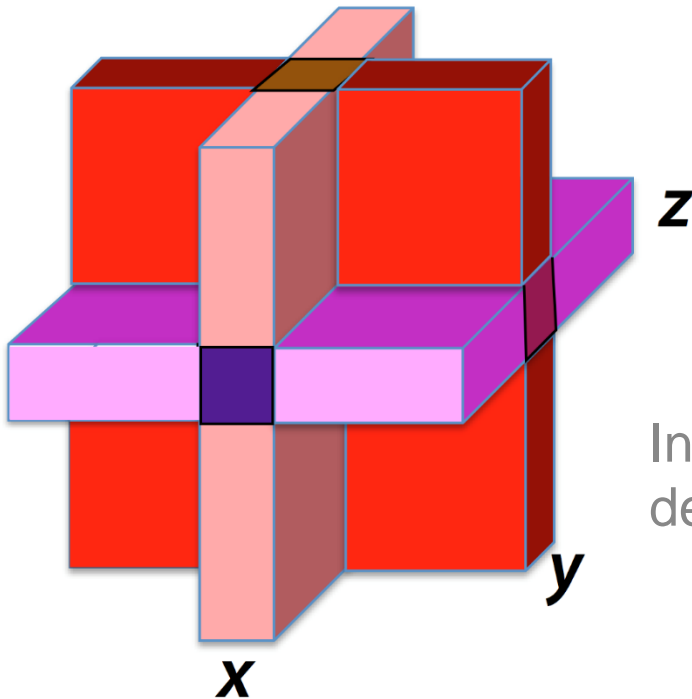
Single-voxel spectroscopy (SVS)



Multi-voxel spectroscopy



Single Voxel Spectroscopy (SVS)



Intersection of 3 orthogonal planes defines a cubic voxel for SVS.

Single Voxel Spectroscopy (SVS)

- Point RESolved Spectroscopy (PRESS)
- $(90^\circ-180^\circ-180^\circ)$

- Stimulated Echo Acquisition Mode (STEAM)

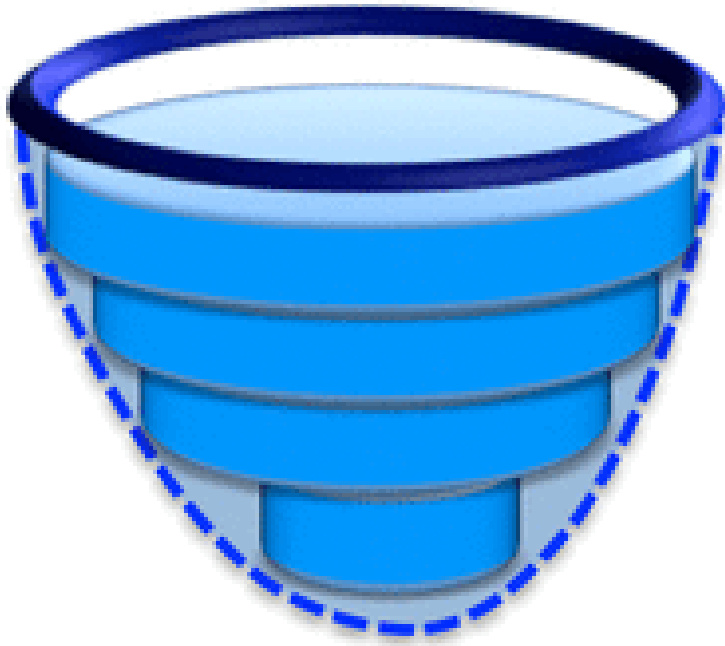
- Image-Selected In vivo Spectroscopy (ISIS).

(Multi-Voxel) Chemical Shift Imaging (CSI)

- 1D (a column of voxels), 2D (a plane of voxels), or 3D (block of voxels).
- parallel imaging,
- reduced k -space sampling,
- multi-band excitation
- *Turbo Spectroscopic Imaging (TSI)*,

	Single Voxel (SVS)	Multi-voxel (CSI)
Operator set-up	Fast and easy	A little harder and slower
Shimming	Limited volume of interest allows very good shim to be obtained	Difficult to shim well over entire region
Spectral quality and peak separation	Excellent with high signal-to-noise, quantifiable	Lower signal-to-noise, problems with quantification
Spectral contamination	From adjacent tissues due to partial volume and chemical shift displacement effects	Bleeding of spectra from adjacent voxels due to chemical shift aliasing
Imaging time	Fast (3-5 min per voxel)	Slower, depends on resolution: 5-8 min for 2D, 7-15 min for 3D
Suitability based on size/ characteristics of lesion	Best for medium-sized homogeneous lesions in large organs	Best for lesions in small organs or for inhomogeneous lesions in larger organs

Surface Coil Localization



Surface coil localization
combining sensitive
volume with 1D CSI

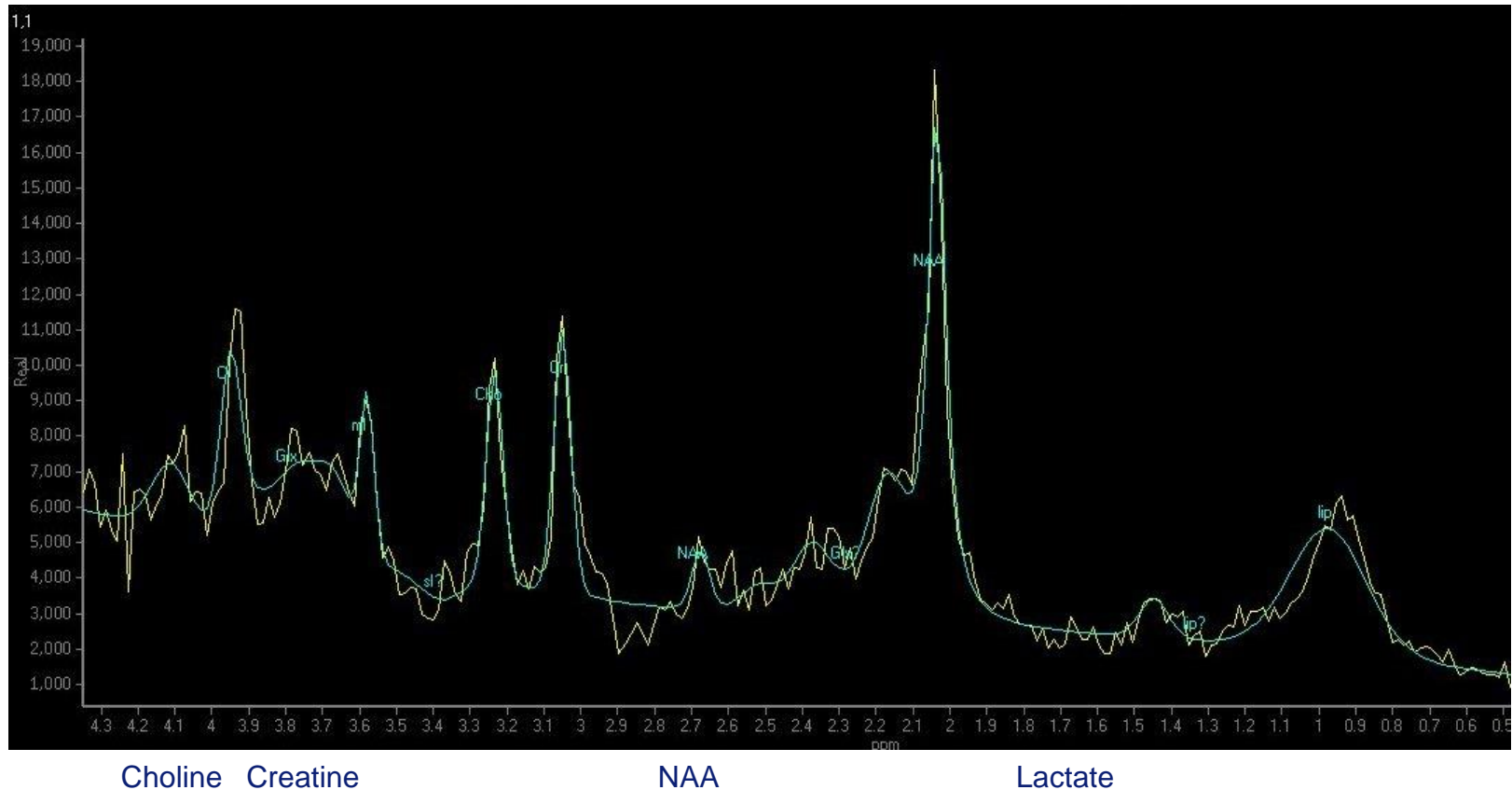
Method	Description	Comments
PRESS (Point RESolved Spectroscopy)	90°–180°–180° slice-selective pulses applied together with orthogonal gradients; generates spin echo (SE) signal at their intersection	Overwhelmingly most popular method for ¹ H MRS; can be used for both single and multi-voxel studies; minimum <i>TE</i> is limited due to multiple RF pulses, so not suitable for short T2 metabolites
STEAM (Stimulated Echo Acquisition Mode)	90°–90°–90° slice-selective pulses applied together with orthogonal gradients; generates stimulated echo (STE) signal at their intersection	Because STE's are recorded instead of SE's, STEAM signal is only 50% as large as PRESS; for ¹ H MRS at ≤ 3T, PRESS is now preferred. STEAM does have lower RF-power deposition (since no 180° pulses used), and allows for somewhat shorter <i>TE</i> 's than PRESS.
ISIS (Image Selected In vivo Spectroscopy)	Series of spatially selective 180° adiabatic pulses and orthogonal gradients in various on/off combinations, followed by a non-selective adiabatic 90° pulse with free induction decay (FID) signal detection	Primary use for non- ¹ H MRS applications (esp. ³¹ P) where T2 values may be very short; tolerant to B ₁ field inhomogeneities (major advantage if transmit surface coils are used); can be used for both single and multi-voxel studies; 8 separate acquisitions must be performed for SVS with pairwise addition/subtraction, resulting in motion sensitivity
CSI (Chemical Shift Imaging)	Employs phase-encoding gradients in 1, 2, or 3 directions to segment larger stimulated volume into multiple smaller voxels	Also known as Multi-Voxel Spectroscopic Imaging (MVS _I); may be 1D (column of voxels), 2D (plane of voxels), or 3D (block of voxels), depending on the number of phase-encoding directions used; larger volume is usually excited/defined by (PRESS, STEAM, ISIS) although other methods possible (FID, SE, TSE)
Surface Coil Localization Methods	Use receive and/or transmit properties of local surface coils to define spectroscopic volume	Primarily used for non- ¹ H spectroscopy of superficial organs (esp. ³¹ P MRS of muscle, heart, and liver); whole coil reception without gradients defines hemispherical volume; this can be improved by use of slice-selective depth pulses and phase-encoding (CSI)

LASER (Localization by Adiabatic SElective Refocusing)

- "semi-LASER",
- resemble PRESS
- .., reduce chemical shift artifacts and are more tolerant to B1 inhomogeneities than PRESS or STEAM methods.

Proton spectrum of the brain

¹H Spectrum of human brain:



1H Metabolites

Some typical values @ 1.5T

Metabolite	Chemical Shift (ppm)	T ₁ (ms)	T ₂ (ms)	Concentration (mMol/l)
Tetramethyl silane (TMS) (Reference)	0.0			
Lipids	1.1 - 1.6			
Lactate (Lac)	1.3 - 1.5	1550	1200	-
N-acetyl Aspartate (NAA)	2.0	1450	450	~10
Creatine + Phospho-creatine (Cr + PCr)	3.0	1550	240	6-12
Choline (Cho)	3.2	1150	330	~2
Taurin	3.3	1700	270	-
<i>Myo</i> -Inositol (mIns) + Glycine	3.5	900	110	6.6
Water	4.65			110*10 ³
Tyrosine/Histidine/Tryptolan	6.0 - 7.5			
Cholesterol	6.5 - 8.0			

- ⊕ → head_1H
- ⊕ pediatric_head_1H
- └─ brainhead_1H
- ⊕ prostate Body part: Head
- ⊕ qa_1H
- ⊕ heart_31P
- ⊕ liver_31P
- ⊕ muscle_31P
- └─ qa_31P
- └─ x_nuc_library









- ⊕ Intervention
- ⊕ adjustments
- ⊕ pediatric_head
- ⊕ pediatric_spine
- ⊕ SequenceRegion
- ⊕ USER

- └─ spectroscopy
- ⊕ → head_1H
- ⊕ pediatric_head_1H
- └─ breast_1H
- ⊕ prostate_1H
- ⊕ qa_1H
- ⊕ heart_31P
- ⊕ liver_31P
- ⊕ muscle_31P
- └─ qa_31P
- └─ x_nuc_library
- ⊕ Intervention







Name	Modified
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5_csi_matrix	11/29/2017 2:40:12 PM
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5_csi_TxRx	11/29/2017 2:40:14 PM



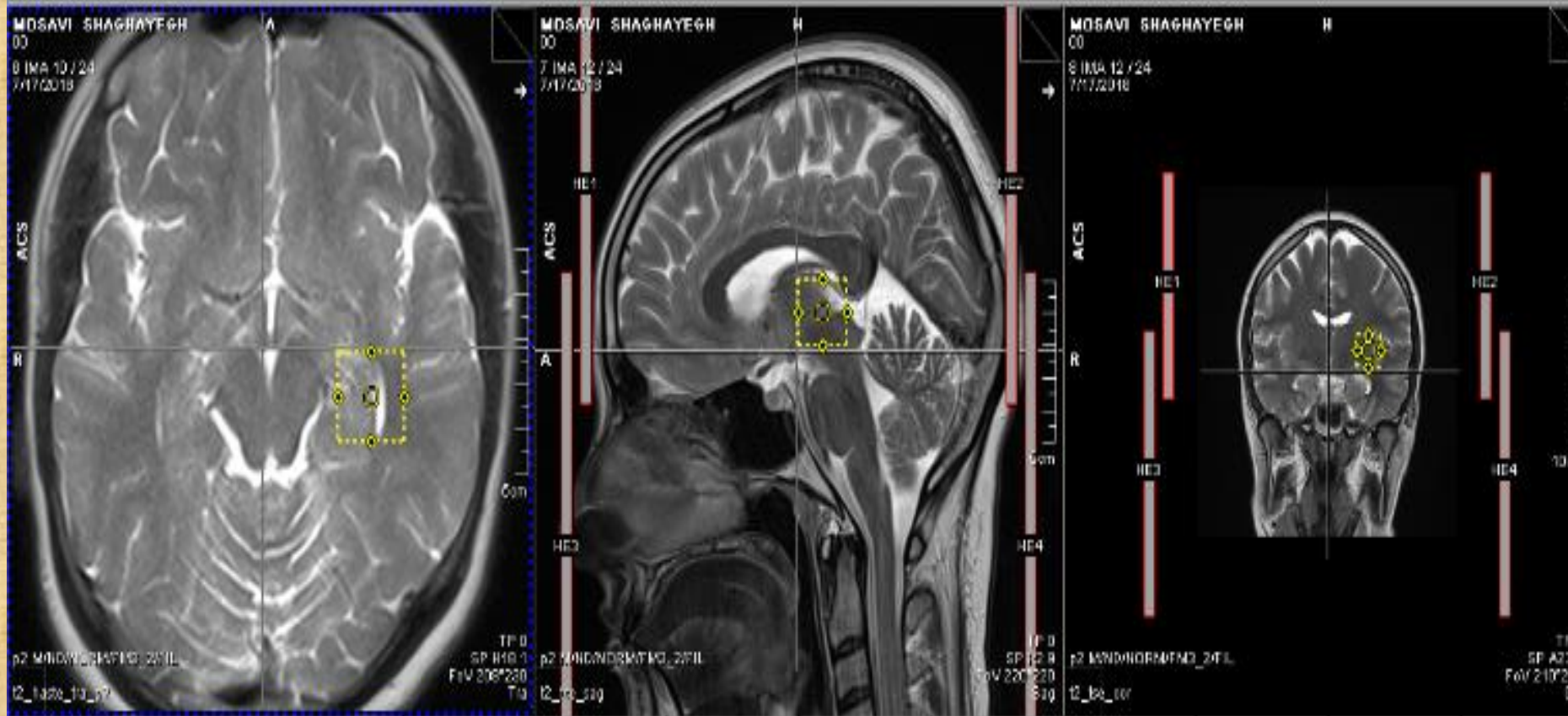
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5_csi_TxRx	11/29/2017 2:40:14 PM

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2		localizer@center	00:09
3		localizer_5	00:40
4		localizer_5@center	00:40
5		sys_se_30	03:20
6		sys_se_135	04:56
7		sys_se_270	07:00
8		sys_st_20	06:32
9		sys_st_135	06:32
10		sys_st_270	06:32

1		localizer	00:09
2		localizer@center	00:09
3	🌸	localizer_5	00:40
4	🌸	localizer_5@center	00:40
5	🌸	localizer_in-plane_csi	01:26
6	🌸	loc_in-plane_csi@center	01:26
7	🌸	csi_se_30	07:12
8	🌸	csi_se_135	07:12
9	🌸	csi_se_270	07:12
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11	🌸	csi_st_20	07:12
12	🌸	csi_st_135	07:12
13	🌸	csi_st_270	07:24

5		sys_se_30	03:20
6		sys_se_135	04:56
7		sys_se_270	07:00
8		sys_st_20	06:32
9		sys_st_135	06:32
10		sys_st_270	06:32

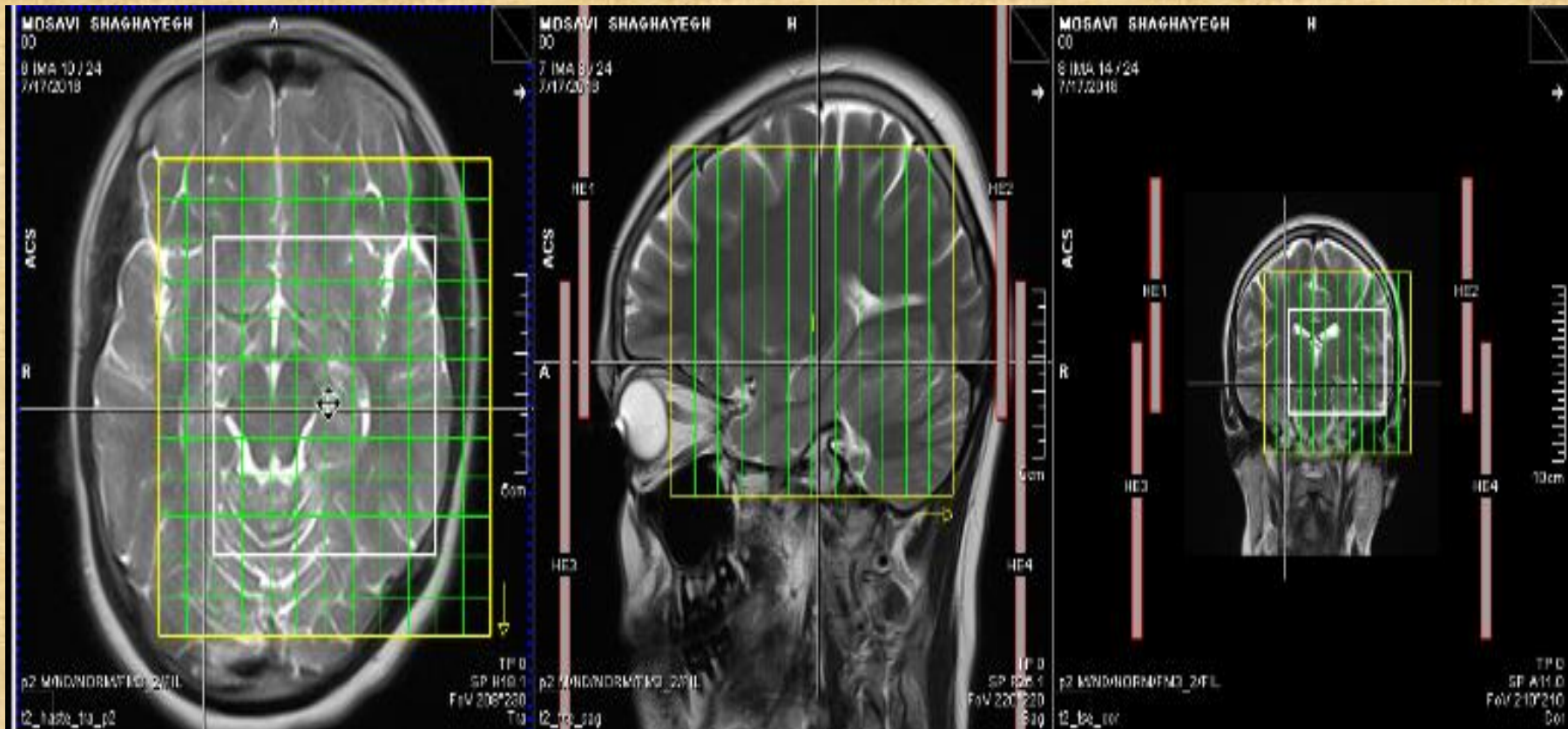
SVS_se

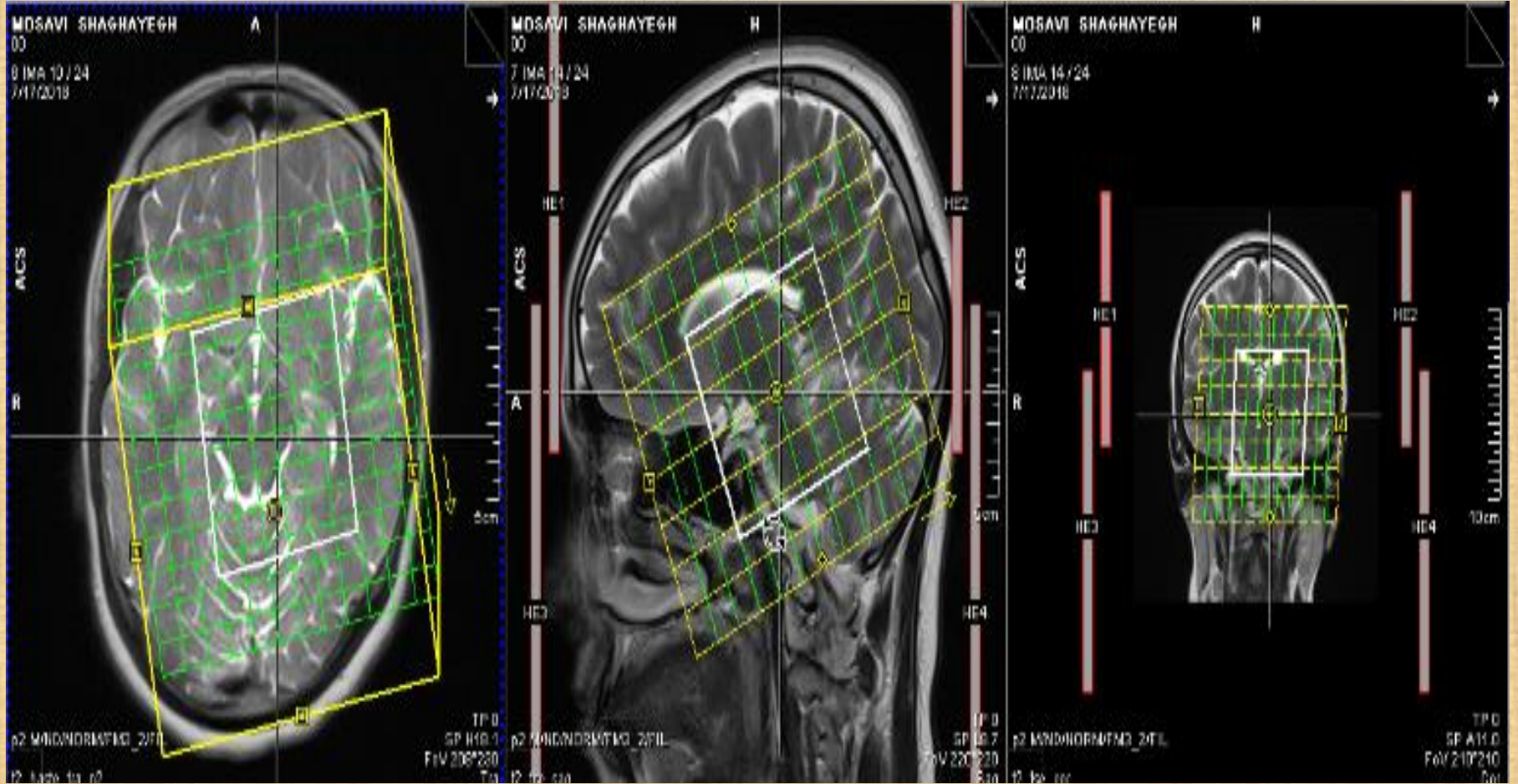


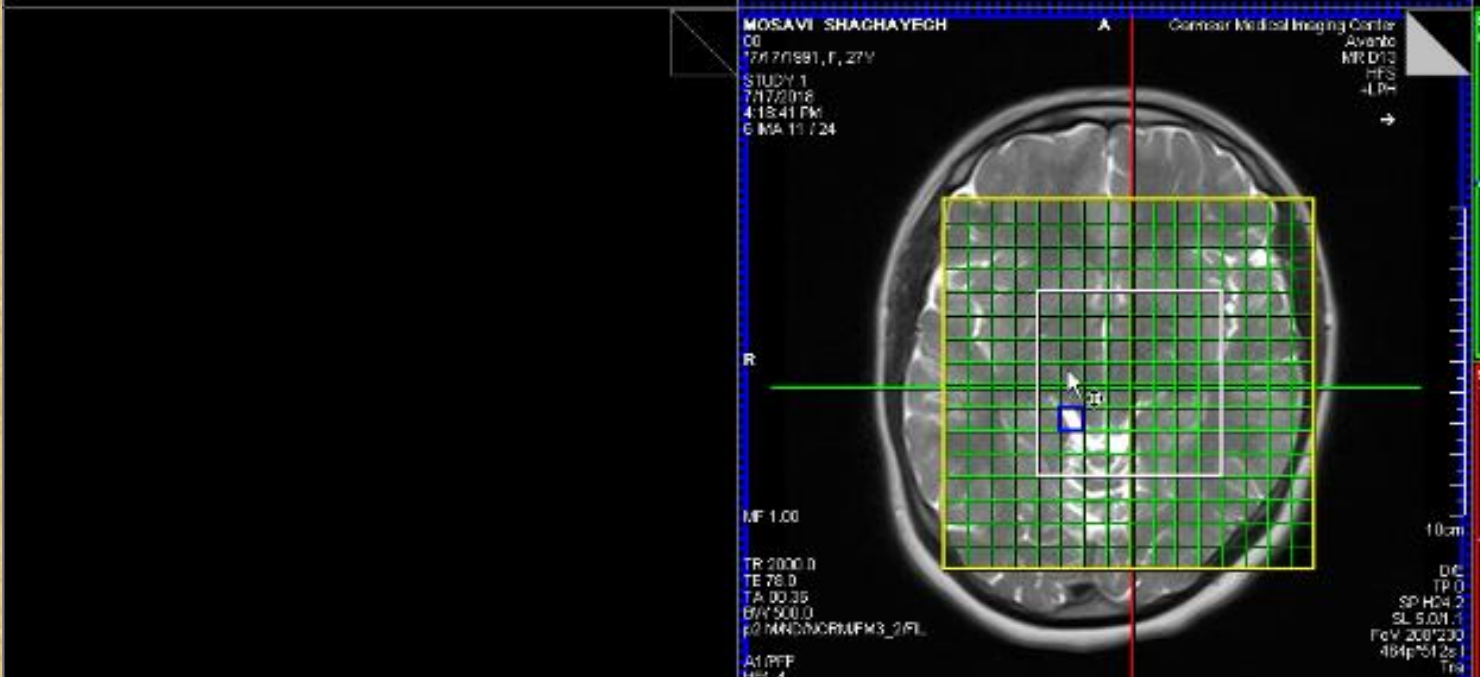
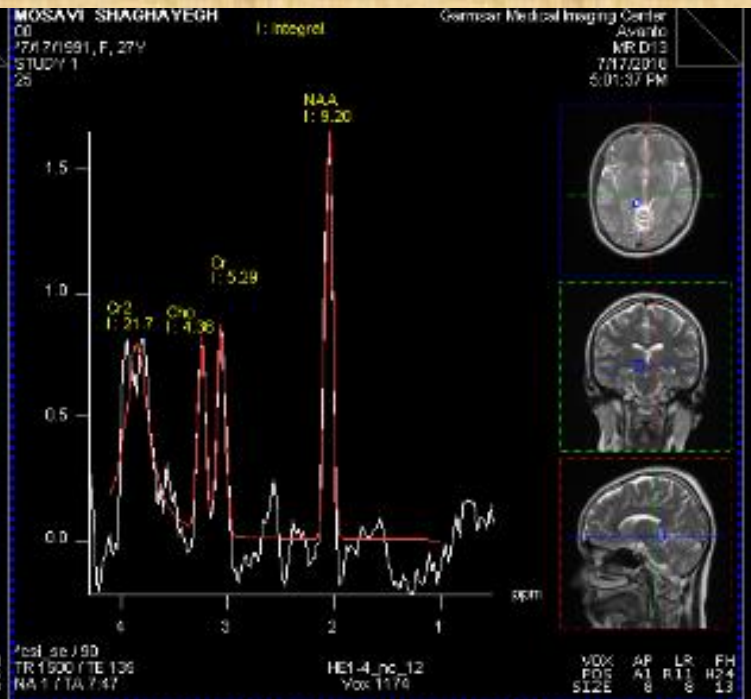
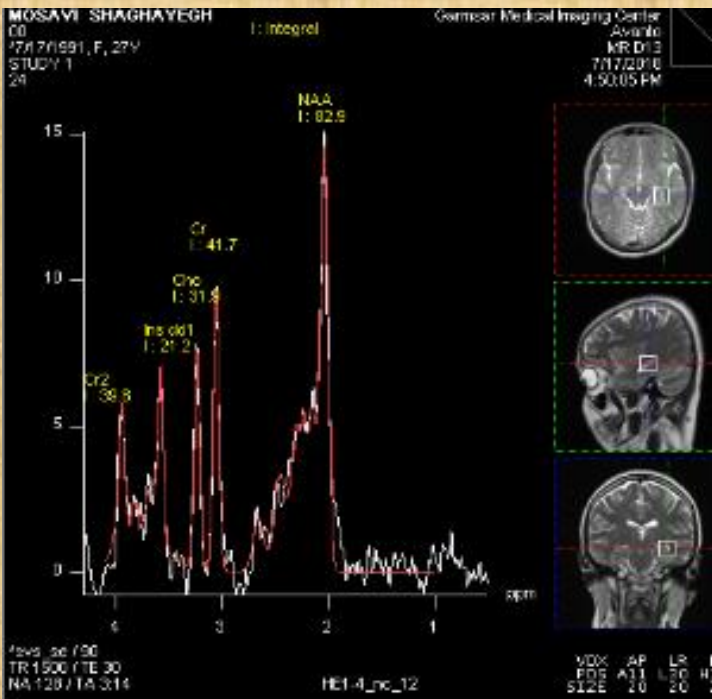
SVS

The image displays a medical imaging software interface with three main scan views and a central dialog box. The top-left view is an axial T2-weighted MRI scan of the brain, labeled 'MOSAVI SHAGHAYEGH 00' and '0 IMA 10 / 24 7/17/2018'. The top-middle view is a sagittal T2-weighted MRI scan, labeled 'MOSAVI SHAGHAYEGH 00' and '7 IMA 8 / 24 7/17/2018'. The top-right view is a coronal T2-weighted MRI scan, labeled 'MOSAVI SHAGHAYEGH 00' and '8 IMA 14 / 24 7/17/2018'. A central dialog box titled 'Confirm Frequency Adjustment' is overlaid on the scans. It features a plot of 'Mag' (Magnitude) versus 'f [Hz]' (Frequency). The plot shows a single sharp peak at approximately 63,629,975 Hz. The plot's x-axis ranges from 63,627,416 to 63,632,524 Hz, and the y-axis has a maximum value of 124,021. The FWHM (Full Width at Half Maximum) is 11.6 Hz. Below the plot, there are two dropdown menus: 'Coil' set to 'Combined' and 'ADC' set to '-'. Below these are two input fields: 'Frequency (sys) [Hz]' and 'Frequency (temp) [Hz]', both containing the value '63629975'. An 'Apply' button is located at the bottom right of the dialog box. At the bottom of the interface, there are three small thumbnail images of the brain scans and the text 'MOSAVI SHAGHAYEGH 7/17/2018'.

CS-3D-se-



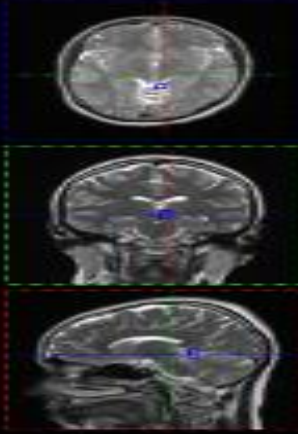
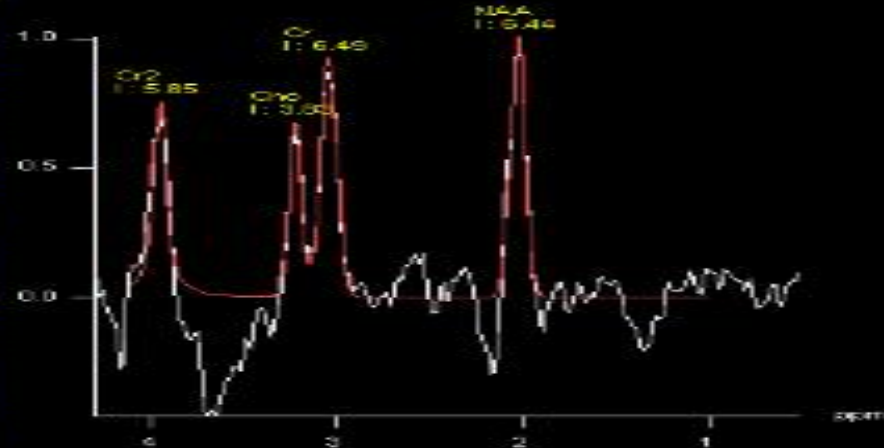




MOSAVI SHAGHAYEGH
00
17/11/1991, F, 27Y
STUDY 1
20

I: Integral

Compass Medical Imaging Center
Avalon
MR D10
7/17/2018
5:01:37 PM



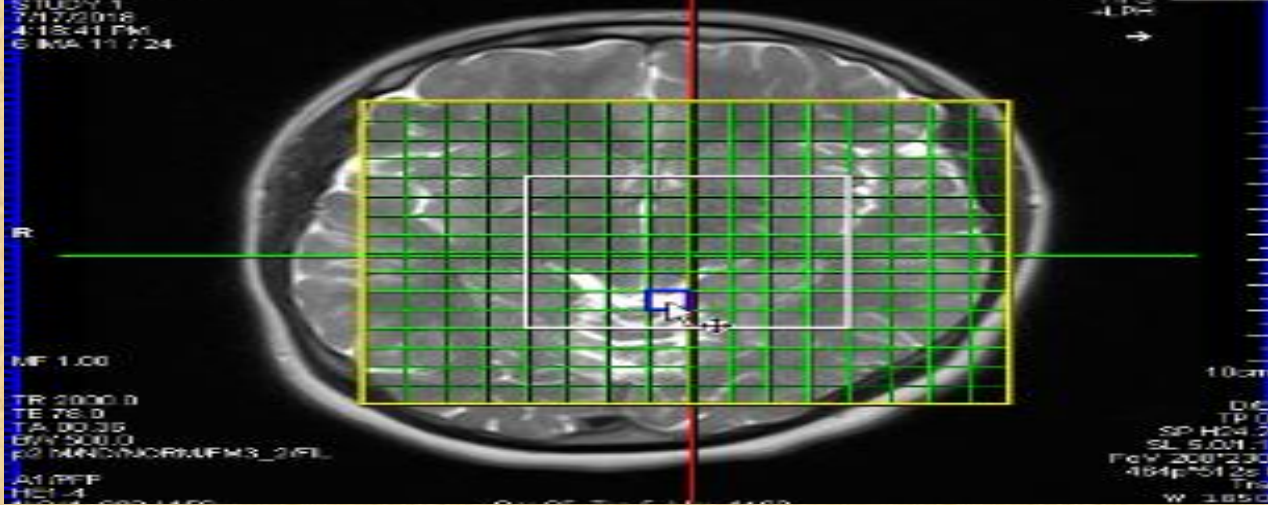
7591 25790
TR 1500 / TE 136
NA 1 / TA 7.47

HE1-4_NX_12
Vox 1182

5.85
3.05
1.64
L
R
P
A

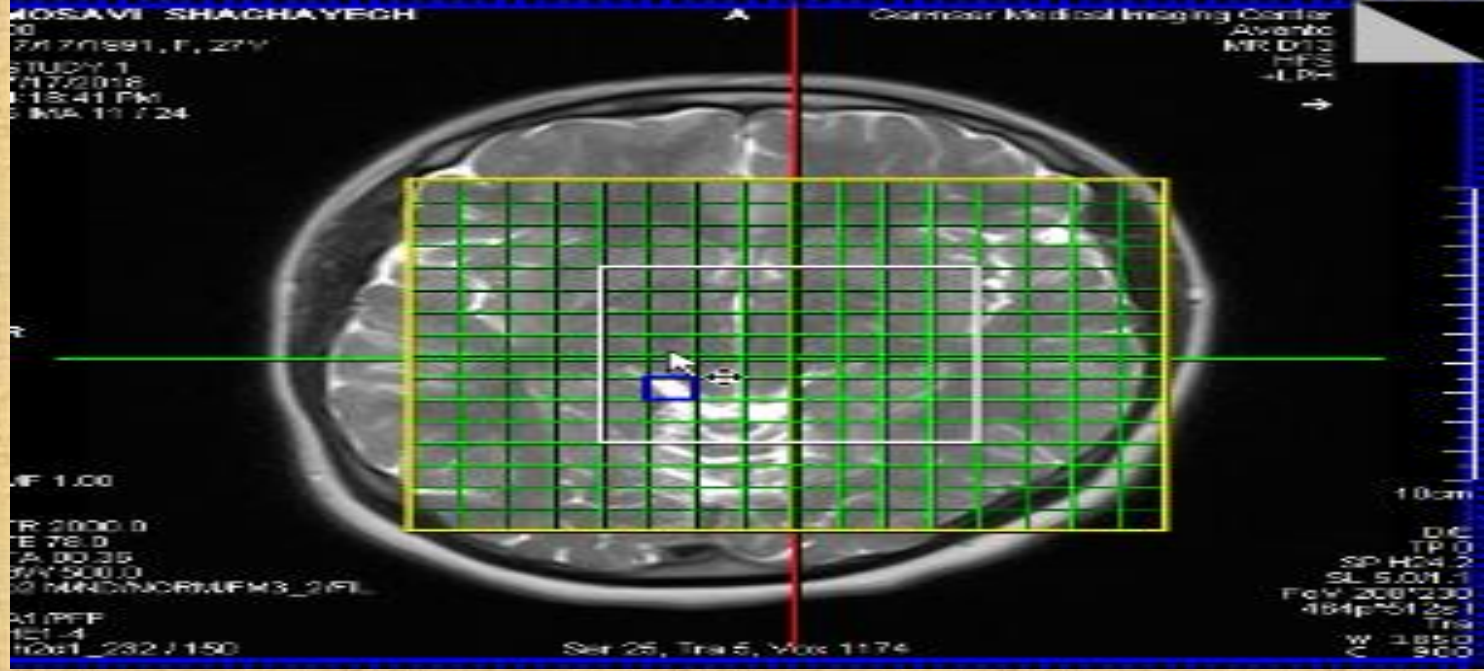
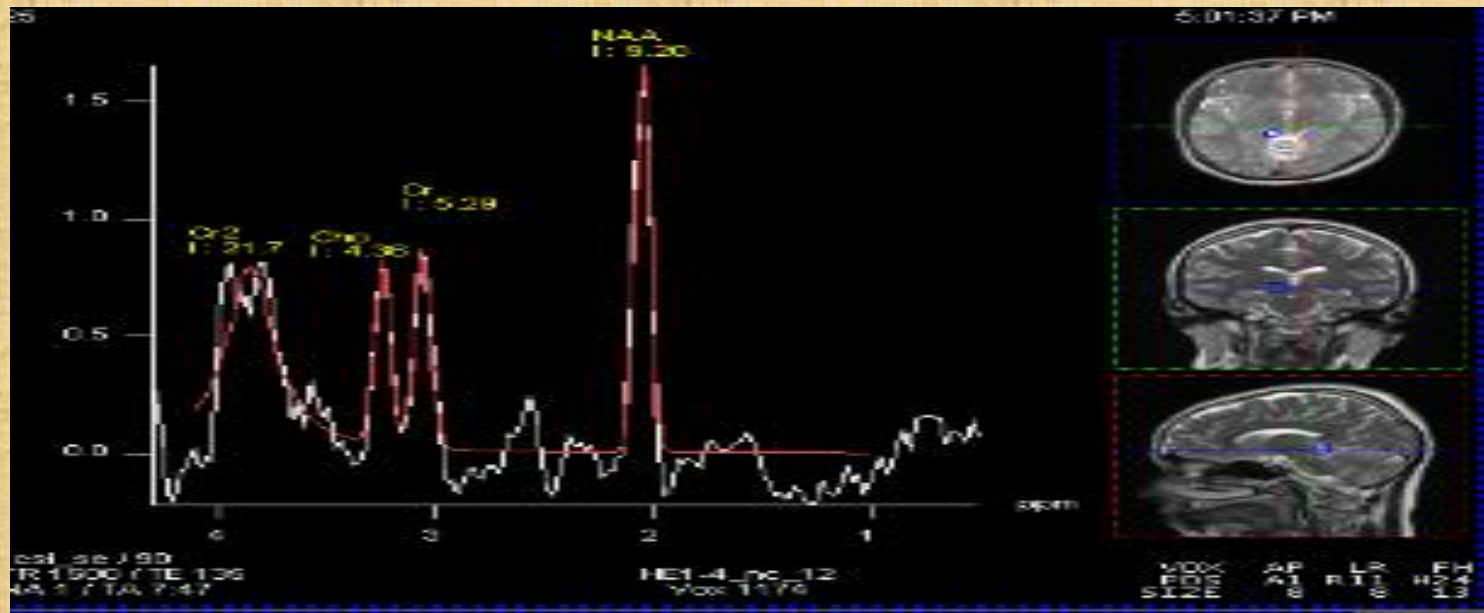
MOSAVI SHAGHAYEGH
00
17/11/1991, F, 27Y
STUDY 1
7/17/2018
4:15:41 PM
C:MA 11/7/24

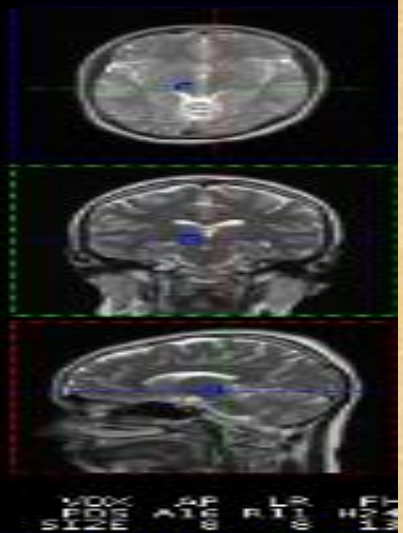
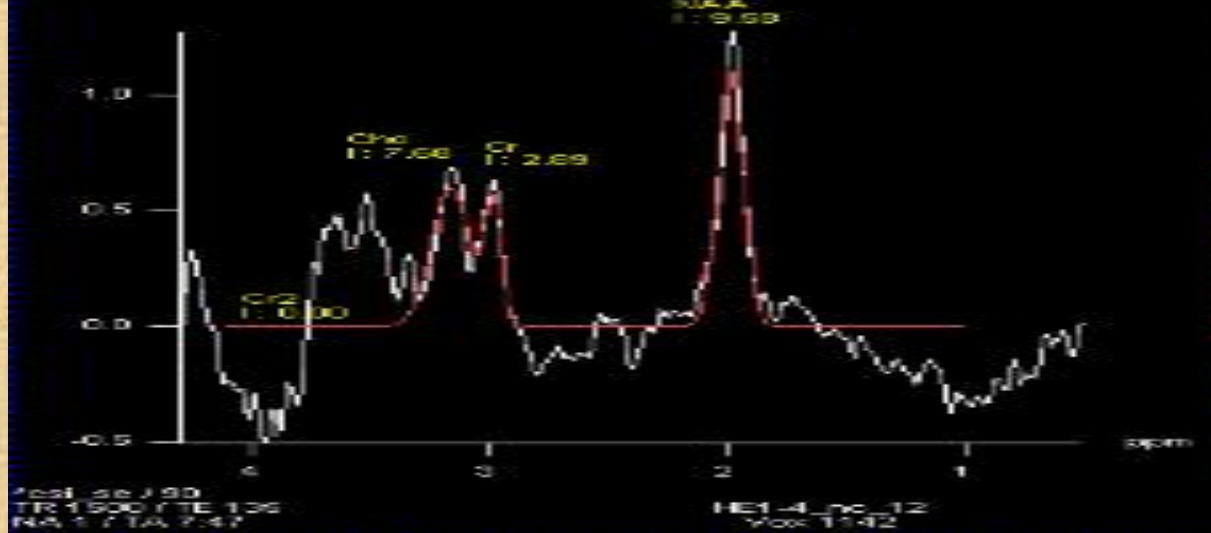
Compass Medical Imaging Center
Avalon
MR D10
7/17/2018
4:15:41 PM



MF 1.00
TR 2000.0
TE 75.0
FA 90.35
DYN 200.0
F0 M4C0NORMEM3_2/FL
A1 PFP
HE1-4

D6
TP 0
SP H24.0
SL 5.001
Fov 200.0
484P
W 3850





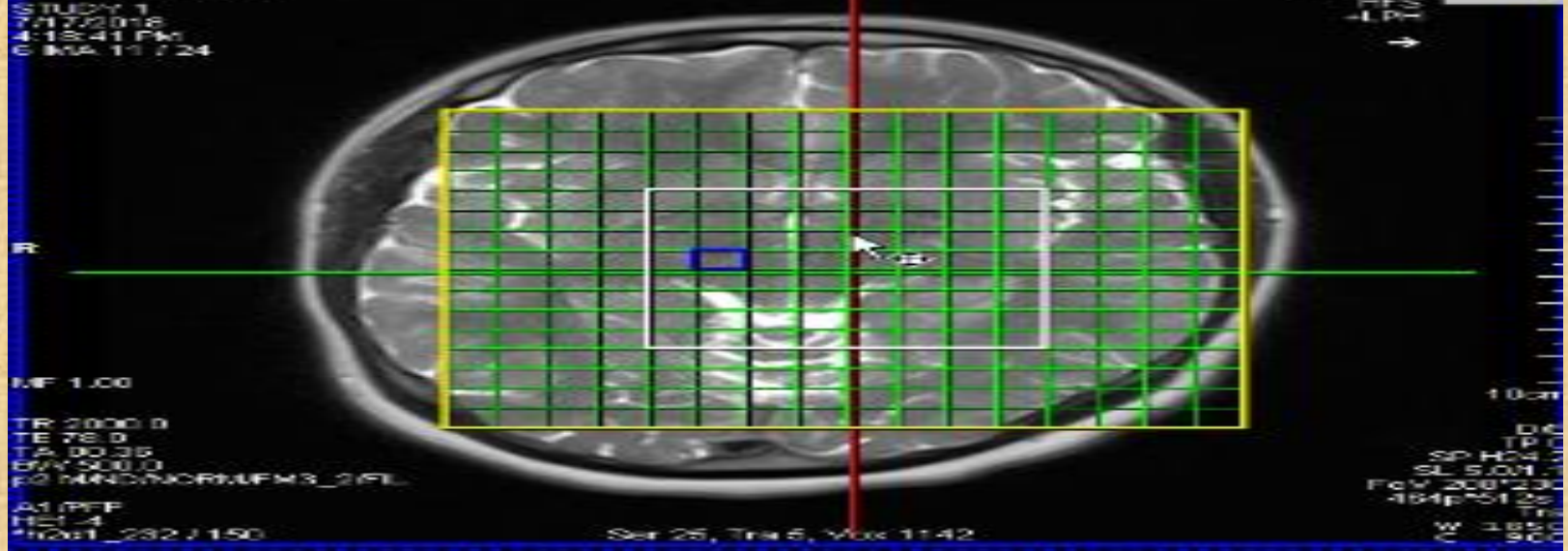
7.06 2.89 1.95
 TR: 1500 TE: 136
 RA: 17.1A 7.47

HE1_4_Vox_12
 Vox: 1142

5 HV 100 max A 15 R L (0-0) H 15

MOSAVI SHAGHAYECH
 DOB: 17/7/1991, F, 27Y
 W TUDY: 1
 4:21:41 PM
 6:00:11:24

Geemar Medical Imaging Center



MF: 1.00
 TR: 2000.0
 TE: 78.0
 TA: 00.36
 SFO: 500.0
 FO: MIND_NORMEM3_2FL
 A1: PRF
 HE1_4
 *tr01_232 / 150

Ser 25, Tra 5, Vox 1142

10cm
 DICOM
 TP: 150
 SP: 150
 SL: 5
 FOV: 230.0
 464p
 W: 1850
 H: 900

3	ACT	Calibration	00:07
4	RxD	AX FLAIR FS	00:08
5	RxD	Ax T2 FSE	02:43
6		Ax T1 memp	01:23
7		Ax DWI 1000b *OPTIO...	01:49
8		Sag T1 CD+	
9		COR T1 fatsat CD+	
10		Ax T1 CD+	
11		PROBE-SV 144	02:43
12		PROBE-SV 35	
13		PROBE-SV 144	
		PROBE-SI 144	04:20

Auto Scan



Head First, Supine

2D T2flair
 EDR, TRF, Fast, ARC
 Coil: BHRBRAIN



AX FLAIR FS

GRX

2:43

Scan Plane: Axial

Freq FOV: 23.8

Phase FOV: 0.00

Slice Thickness: 4.0

Spacing: 1.0

S/I: 172.0

L/R: 0.0

P/A: 010.0

Start: 172.0

End: 180.0

Chem SAT: Fat

Contrast:

Total # Slices: 28
 Max # Slices: 10
 # of Acqs: 3
 Ref: 1000



AX FLAIR FS

GRX

2:43

Scan Plane: Axial

Freq FOV: 23.8

Phase FOV: 0.00

Slice Thickness: 4.0

Spacing: 1.0

S/I: 172.0

L/R: 0.0

P/A: 010.0

Start: 172.0

End: 180.0

Chem SAT: Fat

Contrast:

Total # Slices: 28
 Max # Slices: 10
 # of Acqs: 3
 Ref: 1000



Done	Description	Time
1	3-Plane Loc	00:07
2	Calibration	00:06
3	ACT: AX FLAIR FS	02:43
4	RxD Ax T2 FSE	01:23
5	RxD Ax T1 memo	01:49
6	InRx Ax DWI 1000b *OPTI...	01:00
7	Sag T1 CD+	02:43
8	COR T1 fairsat CD+	04:20
9	AX T1 CD+	
10	PROBE-SV 144	
11	PROBE-SV 3S	
12	PROBE-SV 144	
13	PROBE-SI 144	

Ax DWI 1000b *OPTI* GRx Cx

Scan Plane: **Oblique**

Fix FOV: **26.0** Fix Dir: **R/L**

Phase FOV: **3.0** TR: **1190.0**

Slice Thickness: **3.0** # Slices: **24**

Slicing: **3.0**

R/L A/P S/I

Start: **L0.3** **A15.3** **S0.3** Total # Slices: **24**

End: **R4.3** **P25.0** **S0.3** # of Axes: **3**

Res: **512x512** **70**

Chem SAT: **None**

Contrast

Save Rx



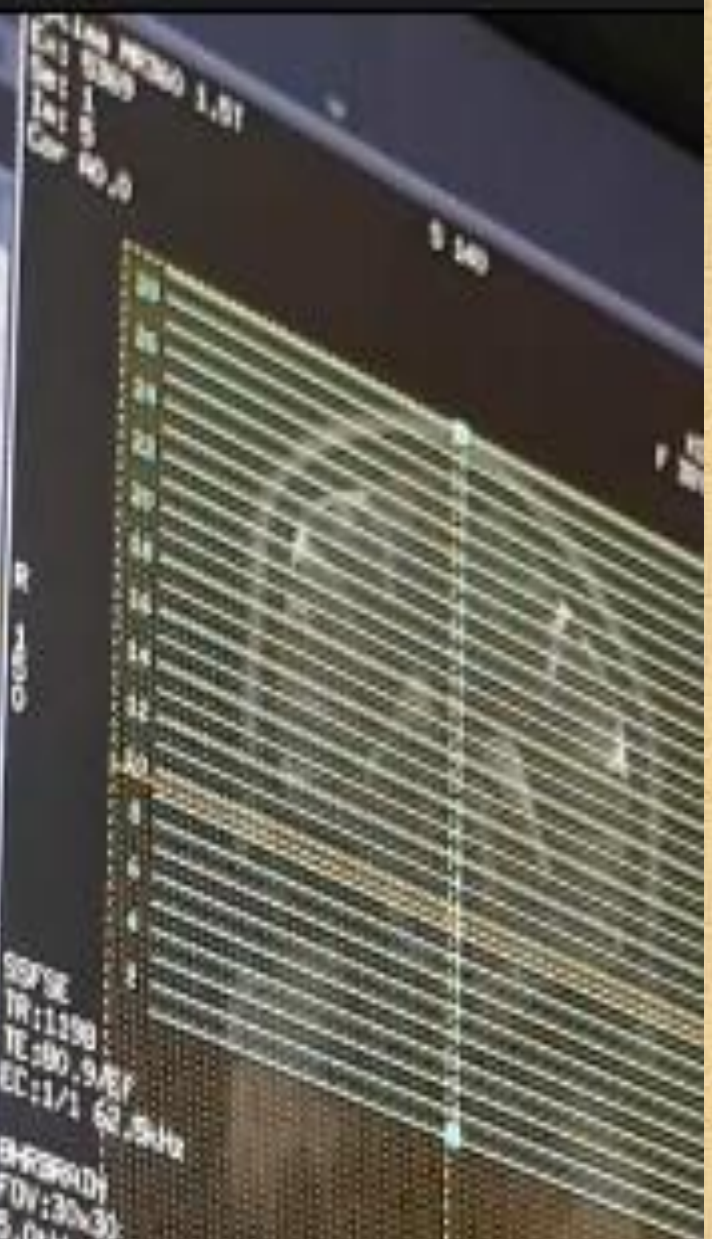
Imaging Options...

- 2D Spin Echo
- EPI, DIFF, Asset
- Coil: BHRBRAIN

SAR Est: 0.23 PPAR: 0.46 E-RMS: 1.20uT Mode: Fast

1:48 PM

Step	Description	Time
1	Done 1 3-Plane Loc	00:02
2	Done 2 Calibration	00:06
3	Done 3 Ax FLAIR FS	02:43
4	Done 4 Ax T2 FSE	01:23
5	Done 5 Ax T1 memo	01:49
6	ACT 6 Ax DWI 1000b *OP...	01:00
7	RxD Sag T1 GD+	02:09
8	RxD COR T1 falsat GD+	01:57
9	RxD Ax T1 GD+	03:04
10	PROBE-SV 144	
11	PROBE-SV 35	
12	PROBE-SV 144	
13	PROBE-SI 144	



10	AX T1 CD+	02:09
11	PROBE-SV 144	01:57
12	PROBE-SV 35	03:04
13	PROBE-SV 144	
	PROBE-SV 144	
	PROBE-SV 144	
	Setup	
	Add Task	04:20



- Done 2 3-Plane Loc 00:27
- Done 3 Calibration 00:36
- Done 4 AX FLAIR FS 02:43
- Done 5 Ax T2 FSE 01:23
- Done 6 Ax DWI 1000b *OP... 01:49
- Done 7: Sag T1 CD+ 01:00
- ACT 8: COR T1 fatsat CD+ 02:09
- RxD Ax T1 CD+ 01:57
- InRx PROBE-SV 144 01:37
- PROBE-SV 35 03:48
- PROBE-SV 144 03:48
- PROBE-SI 144 04:20

Setup Add Task ▶ Run

View

Auto Scan

Start

Save Rx



Imaging Options...

MRS Probe-P
EDR
Coil: 8HBRRAIN

PROBE-SV 144 GRX 3:48

Scan Plane: Axial

Freq. FOV: 24.0

Voxel Thickness: 19.9

CSI Slice Thickness: 20.0

Center: (20.2, 132.7, A28.7)

Length: 19.9, 20.0, 20.0

Z X Y

Center/Len: Start/End

Chem SAT: None SAT LABALI

Contrast

- Done < Calibration 02:43
- Done 3: AX FLAIR FS 01:23
- Done 4: Ax T2 FSE 01:49
- Done 5: Ax T1 memo 01:00
- Done 6: Ax DWI 1000b *D... 01:57
- Done 7: Sag T1 GD+ 01:37
- Done 8: COR T1 falsat GD+ 01:37
- Done 9: Ax T1 GD+ 03:48
- Done 10: AX T2* GRE 03:48
- 11 InRx PROBE-SI 144
- 12 PROBE-SV 144
- 13 PROBE-SV 35
- 14 PROBE-SV 144

Setup View Run

Add Task ▶

Auto Scan

Scan

Save Rx



Imaging Options...

MRS Probe - P
EDR
Coil BHRBRAIN

PRIME PROBE 1.5T

SE: 8
T1: 11
Cap: MAG.1

0 300

PROBE-SI 144

1 126

420

Scan Plane: Axial

Freq: TOV 13.0

Voxel Thickness: 20.0

CSI Slice Thickness: 20.0

Freq Off: A/P

TR: 1000.0

CSI Slices: 1

Start: 13.0 13.0 13.0

End: 10.0 10.0 10.0

Chem SAT: None

Max # Slices: 16

of Apps: 1

Rel ShdW: 12%

Contrast

SAR Est: 0.33 PrAc: 0.65 R-RMS: 1.56uT Mode: First